

**Amendments to the Specification:**

Please modify the paragraph at page 8, lines 2-17 in the following manner:

Accordingly, by excessively acquiring echo signals in the low spatial frequency regions alone, it is possible to acquire echo signals for data distribution data for each unit region and each receiver coil unit simultaneously with measurements of echo signals for image reconstruction. Hence, sensitivity distribution data of each receiver coil unit can be acquired in responding to body motions of the subject being imaged with a slight extension of the imaging time. In particular, in a case where extracting and synthesizing of echo signals in the low spatial frequency regions in the respective unit regions as described above is not sufficient to find the sensitivity distribution data, by measuring echo signals densely in the low spatial frequency region in one or more ~~blades~~ unit regions, echo signals for sensitivity distribution data can be acquired at a sufficiently high density to find the sensitivity distribution data.

Please modify the paragraph at page 15, lines 5-11 in the following manner:

Also, according to one preferred aspect, the overall control means repeats for each unit region, a measurement of echo signals corresponding to the unit region by the measurement control means, formation of the unit region image using the echo signals by the unit region image forming means, and formation of the entire image from the unit region image and another unit region image by the entire image forming means, ~~are repeated for each unit region.~~

Please modify the paragraph at page 18, lines 6-23 in the following manner:

The gradient magnetic field generating system 3 comprises gradient coils 9 wound around in three axial directions, X, Y, and Z, and gradient power supplies 10 that drive respective gradient coils. It assigns one of a slicing gradient pulse (Gs), a phase encoding gradient

pulse (Gp), and a frequency encoding gradient pulse (Gr) to each of the X-, Y-, and Z-axis directions, and applies these pulses to the subject 1 by driving the gradient power supplies 10 for the respective coils according an instruction from the sequencer 4 described below. To be more concrete, a slice plane is set with respect to the subject 9 1 by applying Gs to one of the X, Y, and Z directions, and Gp and Gr are applied to the remaining two directions to encode position information of the respective directions in echo signals. Alternatively, when a slice plane is oblique, the three gradient magnetic fields are distributed to the respective axial directions depending on the oblique angle, and a sum of the gradient magnetic fields in each axial direction is applied in the corresponding axial direction.

Please modify the paragraph at page 45, lines 3-11 in the following manner:

Also, the parallel MRI method in a case where the number of the RF receiver coil is two and the phase encoding interval is doubled has been described. However, the number of the RF receiver coils and the magnification of the phase encoding intervals can be set arbitrarily (note, however, that the number of RF receiver coils  $\geq$  magnification of phase encoding intervals). In addition, signals acquired at the RF receiver coils can be selected and synthesized to match with a plane being imaged.